Application of an ultraminiature thermal neutron monitor for irradiation field study of accelerator-based neutron capture therapy

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Phantom experiments to evaluate thermal neutron flux distribution were performed using the Scintillator with Optical Fiber (SOF) detector, which was developed as a thermal neutron monitor during boron neutron capture therapy (BNCT) irradiation. Compared with the gold wire activation method and Monte Carlo N-particle (MCNP) calculations, it was confirmed that the SOF detector is capable of measuring thermal neutron flux as low as 10^5 n/cm^2/s with sufficient accuracy. The SOF detector will be useful for phantom experiments with BNCT neutron fields from low-current accelerator-based neutron sources.

Keywords: neutron capture therapy; SOF detector; thermal neutron monitor

INTRODUCTION

Boron neutron capture therapy (BNCT) is a cancer treatment modality whose therapeutic efficacy relies on both the concentration of boron in the tumor and the thermal neutron flux at tumor sites during irradiation. Boron delivery to the tumor is being addressed by current studies on new boron carriers, while a number of techniques for determining boron concentration, either in vivo or in vitro, have been proposed in order to perform neutron irradiation at the time when the boron concentration in both the tumor and healthy tissue are at their optimum levels [1]. Most of the neutron fields currently being used for BNCT clinical trials come from research nuclear reactors that have been modified to accommodate BNCT irradiations. The number of these facilities has increased in recent years, but due to the limited number of reactors that can be converted for medical irradiation purposes, there are still very few available BNCT irradiation facilities. One possible solution to this would be accelerator-based neutron sources (ABNS) that can be constructed in hospitals, similar to those used in conventional radiotherapy. At present, there are many accelerator facilities that can potentially be used for neutron production, but most of them are unable to provide the required neutron flux for BNCT due to their low beam currents. Some recently proposed accelerator systems that are to be used mainly for BNCT address this limitation in the beam current [2].

The evaluation of the neutron field in a BNCT irradiation facility is generally performed by measuring the distribution of the thermal neutron flux and the gamma dose rate that is generated in a water phantom. The current method for determining the thermal neutron flux in reactor-based BNCT is by means of gold wire activation. However, this may not be practically applicable to an accelerator-based neutron source because of the low neutron flux, which would require very long exposure of the gold wire to the neutron beam to get meaningful results. Moreover, using the gold wire activation method in an epithermal neutron beam requires the...
application of correction factors to account for the relatively large cross-section of neutron absorption in $^{197}$Au at ~0.5 eV. Although a relatively precise evaluation of the thermal neutron flux can be obtained from activation of $^{197}$Au by using wires with and without a cadmium cover, this method requires that the thermal neutron flux is $> 10^6$ n/cm$^2$/s.

Several detectors, including the BF$_3$ counter, fission chamber, Li-doped semi-conductor detectors (e.g. miniature Si detectors with fission converter U-235, MOSFET paired detectors with one of them covered by a B-10 converter, p-in Si diode response), and self-powered neutron detectors can also be used to measure the thermal neutron flux in BNCT [3–6]. Recently, a Scintillator with Optical Fiber (SOF) detector has been developed for real-time thermal neutron flux monitoring during BNCT irradiation [7, 8]. The SOF detector system can easily perform dose profile measurements in a water phantom. More importantly, because it is equipped with a small probe, it is able to perform measurements in conditions inaccessible for other neutron detectors, (e.g. in very narrow spaces). While theoretical evaluation of BNCT neutron fields may now be carried out with reasonable accuracy via a number of simulation codes, for example the Monte Carlo N-particle (MCNP) transport code [9], actual measurements with these detectors are necessary for verifying the validity of these calculations and for routine checks that need real-time data.

We report here the results of experimental validation of the feasibility of implementing the SOF detector system in accelerator-based BNCT. The SOF detector was benchmarked against the results of MCNP calculation and gold wire-activation measurements.

**MATERIALS AND METHODS**

**SOF detector**

Figure 1 is a schematic illustration of the SOF detector, the components of which included a probe with a small amount of plastic scintillator, a plastic optical fiber, a photo-multiplier tube, a charge pre-amplifier, a discriminator and a counter. The plastic scintillator (Bicron BC490, partially polymerized plastic scintillator), which was mixed with a small amount of LiF powder (enriched 95% $^6$Li), was attached to the tip of the plastic optical fiber (Mitsubishi Rayon MH4002, 1 mm-diameter optical fiber with 2.2 mm-diameter polyethylene shielding). The signal recorded by the SOF detector came from the reaction between the $^6$Li nuclei and the thermal neutrons that emitted charged particles (alpha and triton), which in turn produced scintillation photons in the plastic scintillator. The photon signals were transmitted through an optical fiber to the Photon Counting Head (Hamamatsu H7155), which was made up of the photo-multiplier tube, charge pre-amplifier and discriminator. These signals were converted into 30 ns-width TTL pulses, which were sent to a personal computer via a USB (Universal Serial Bus) connection for data processing. The SOF detector system was composed of two identical SOF detectors, one with $^6$LiF and the other without $^7$LiF (for gamma-ray and fast-neutron compensation).

The calibration for estimating absolute thermal neutron flux was performed using a gold activation method used at the JRR-4 research reactor of the Japanese Atomic Energy Agency (JAEA). The conversion coefficient from the SOF count rate to thermal neutron flux was calibrated as $3.69 \times 10^3$...
Accelerator-based neutron source

In this study, neutrons were generated using a Shenkel type single-end accelerator at the Hiroshima University Research Accelerator (HIRRAC), where the maximum accelerator voltage is 3 MV and the maximum beam current of H⁺ is 1 mA. A lithium metal target with a diameter of 25 mm and a thickness of 300 μm was used for neutron production via the $^7$Li$(p,n)$ reaction. While the maximum attainable beam current of HIRRAC is 1 mA, the stable beam current achieved on the day of the experiment was only 50 μA; the HIRRAC beam current is highly dependent on the accelerator condition. With a pure lithium metal target at an accelerator voltage of 2.5 MV, the neutron production rate was $\sim 8.83 \times 10^{11}$ n/s/mA, which corresponds to a neutron production rate at the lithium target of $\sim 4.42 \times 10^{11}$ n/s for 50 μA [10].

Thermal neutron flux measurements

One of the indicators of whether a neutron irradiation field will be suitable for BNCT is the thermal neutron flux distribution it generates in a water phantom. Currently, BNCT clinical studies are mainly performed for brain tumors; therefore, the evaluation of the accelerator-produced neutron beam was carried out using a cylindrical water phantom having dimensions similar to a human head under BNCT irradiation. An 18 cmφ (diameter) × 20 cm (length) cylindrical water phantom constructed from a 3 mm-thick polymethyl methacrylate (PMMA) material was used in the experiment. Figure 2 illustrates the setup for measuring the thermal neutron flux distribution in the water phantom with the SOF detector system. The water phantom was placed behind a 20
cm\(\phi\) (diameter) \(\times\) 20 cm (length) \(\text{D}_2\text{O}\) moderator enclosed in 1-mm-thick stainless steel. The detector probe was set at desired positions in the water phantom using a positioning device controlled by a stepper motor. Thermal neutron flux measurements using the SOF detector were performed at 2.5-mm increments from the inside surface of the phantom up to 20 mm from the outside surface of the phantom, then at 5-mm steps from 20 mm to 50 mm, and at 10-mm increments from 50 mm to 150 mm. Each measurement was performed until the accumulated proton charge was \(5 \times 10^{-3}\) coulomb (i.e. taking \(~100\) s). The scanned direction was along the beam axis, which was defined as the depth direction in this paper.

The data obtained using the SOF detector were compared with estimated values from gold wire activation measurements. The thermal neutron flux distribution was obtained via the cadmium difference method using 0.7-mm gold wires, with and without cadmium covers (i.e. 0.5-mm thick cadmium tubes). The gold wires were placed along the water phantom central axis from the inside surface of the phantom. The gold wire and cadmium tube (which contained gold wire) were taped onto a 2-mm-thick PMMA plate to fix them as exactly as possible at the central beam axis. The first 15 mm, i.e. 5 to 20 mm from the outside surface of the phantom, were separated into six pieces (2.5 mm each), the next 25 mm (20 to 45 mm) into five pieces (5 mm each), and the last 60 mm (45 to 105 mm) into six pieces (10 mm each). The middle position of each gold wire was plotted as the measured position in later figures.

**MCNP calculation**

In order to investigate whether the SOF measured data agreed with calculated data, MCNP simulations were carried out using a calculation geometry based on the experimental set-up shown in Fig. 2. The walls around the irradiation room were included in the calculation geometry because the irradiation room was small enough such that scattered neutrons from the walls were expected to have an appreciable contribution to the SOF measured signals. Neutron production via the \(^7\text{Li}(p,n)^7\text{Be}\) reaction was calculated using the Fortran program LIYIELD.FOR developed by Lee et al. [10]. Here, a proton beam having a Gaussian energy distribution \((\sigma = 0.1\) MeV\) and an average energy of 2.5 MeV was assumed to be incident on a pure lithium metal target with a diameter of 2.5 mm and a thickness of 300 mm. The thickness of the lithium target was chosen such that it would be sufficient to completely stop an incident 2.5-MeV proton.

The neutron flux at the scintillator layer of the SOF detector probe with \(^6\text{Li}\) was obtained using the MCNP with more accurate modeling of the \(^6\text{Li}(n,\alpha)^3\text{H}\) reaction. The same method was used for the calculation of the activation of \(^{197}\text{Au}\). The ENDF-B/VI cross-section library was used in the MCNP calculation.

**RESULTS AND DISCUSSION**

Figure 3 illustrates the measured thermal neutron flux using the gold wire activation method and the SOF detector. The vertical axes in this figure correspond to the actual measured thermal neutron flux (right-hand side scale) and the thermal neutron flux normalized per 1 mA of current (left-hand side scale). The data shown for the gold activation measurement are those with cadmium corrections. Error bars for SOF are not indicated in Fig. 3 because the statistical error for the measurements was at most 0.16%. A discrepancy between the data obtained using the gold wire activation method and the SOF detector is observed in Fig. 3. Here, the gold wire activation method appears to have recorded higher fluxes at shallower depths and lower fluxes at deeper parts of the phantom compared with those obtained by the SOF detector. One possible reason for this discrepancy is the self-shielding in the gold wire due to its diameter (0.7 mm\(\phi\)), which was chosen in order to gain a higher efficiency of detecting thermal neutrons. On the other hand, self-shielding was not expected in the SOF detector.

In order to clarify this difference in the measured neutron flux, MCNP calculations were performed, the results of which are provided in Fig. 4. Both the SOF-measured data and the flux distribution obtained from the gold wire measurement without cadmium correction agreed fairly well with their respective MCNP-calculated data. On the other hand, the neutron flux distribution derived by MCNP for the gold wire with cadmium correction data was revealed to have overestimated the corresponding experimental neutron flux. Incidentally, MCNP yielded an almost identical result for the simulated data for the SOF detector and the gold wire with cadmium correction.

The discrepancy between the data obtained from MCNP and from the experiment for the cadmium-covered gold wire could be traced to the difference between the calculation geometry and the actual experimental set-up. In the MCNP calculation, the gold wire and cadmium pipe were assumed...
to be completely straight (i.e. parallel to the phantom central axis); however, this may not have been exactly the case during the experiment. This could have caused the thermal neutron shielding effect around the cadmium pipe to become bigger, leading to a lower thermal neutron flux for the gold wire placed at deeper sites in the phantom.

The $^{10}\text{B}(n,\alpha)^{7}\text{Li}$ reaction rate profile in the phantom is important information for BNCT treatment because this reaction essentially differentiates the dose delivered to healthy or normal tissues and tumors. In Fig. 5, the experimental data obtained by the SOF detector and the gold wire activation method are compared with the calculated $^{10}\text{B}$ reaction rate normalized to the thermal neutron flux. While the SOF detector measurement agreed with the $^{10}\text{B}$ reaction rate, the gold wire activation data under-estimated the $^{10}\text{B}$ reaction rate at central axis depths > 20 mm from the phantom surface. This could have been brought about by the effect of self-shielding, which occurs when relatively thick gold wires (i.e. 0.7 mm in diameter) are used, which would result in a measured thermal neutron flux in deeper parts of a neutron-irradiated medium that is lower the actual value at these depths. With increasing of the depth in water, the ratio of 0.5-eV thermal neutrons to the rest of the neutrons (with lower or higher energies) would change due to moderation of the spectra. The SOF detector can pick up much better moderation of the neutron spectra than Au foil, thus leading to underestimation of Au in a greater depth. It is obvious that the SOF detector is more advanced for BNCT dosimetry, because this detector will provide a response close to B-10.

As demonstrated in Figs 3–5, the SOF detector is capable of accurate thermal neutron flux measurements, even with flux as low as $10^5$ n/cm$^2$/s. For the gold wire method, it will take a few days to measure the thermal neutron flux of $10^6$ n/cm$^2$/s with sufficient accuracy; this is inclusive of the irradiation time and the measurement time. In contrast, it took only 30 min to obtain almost the same data using the SOF detector. This means that the SOF detector system is suitable for phantom experiments to evaluate thermal neutron flux distributions produced by accelerator-based neutron sources, even at low proton beam currents (when low neutron fluxes are expected).

**CONCLUSION**

In this study, in-phantom thermal neutron flux measurements were performed in order to determine the feasibility of using the SOF detector system for the characterization of neutron irradiation fields from an accelerator-based neutron source for BNCT. Neutron flux distribution measured by the SOF detector was compared with that measured using the gold wire activation method and with estimated data from MCNP in order to demonstrate the accuracy of SOF-measured data.

It has been confirmed that the SOF detector is able to measure thermal neutron flux as low as $10^5$ n/cm$^2$/s with sufficient accuracy, as indicated by good agreement between the experimental and calculated data obtained for the SOF detector. Compared with the gold wire activation method, the SOF detector system offers better flux estimation because the activation method requires the use of thick gold wires when measuring neutron flux as low as $10^5$ n/cm$^2$/s, which results in underestimation due to self-shielding.

Finally, this study has demonstrated that the SOF detector system can be implemented in phantom experiments for evaluation of thermal neutron flux distributions generated by accelerator-based neutron sources.

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REFERENCES


